

Neural Dynamics of Event Segmentation in Music: Converging Evidence for Dissociable Ventral and Dorsal Networks

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SUMMARY

The real world presents our sensory systems with a continuous stream of undifferentiated information. Segmentation of this stream at event boundaries is necessary for object identification and feature extraction. Here, we investigate the neural dynamics of event segmentation in entire musical symphonies under natural listening conditions. We isolated time-dependent sequences of brain responses in a 10 s window surrounding transitions between movements of symphonic works. A strikingly right-lateralized network of brain regions showed peak response during the movement transitions when, paradoxically, there was no physical stimulus. Model-dependent and model-free analysis techniques provided converging evidence for activity in two distinct functional networks at the movement transition: a ventral fronto-temporal network associated with detecting salient events, followed in time by a dorsal fronto-parietal network associated with maintaining attention and updating working memory. Our study provides direct experimental evidence for dissociable and causally linked ventral and dorsal networks during event segmentation of ecologically valid auditory stimuli.

INTRODUCTION

Event segmentation is fundamental to object identification and feature extraction. The real world typically presents our sensory systems with a continuous stream of undifferentiated information. In order to make sense of this information, the brain needs to segment or chunk the incoming

stimulus stream into meaningful units; it accomplishes this by extracting information about beginnings, endings, and event boundaries from the input. Studying event segmentation in real-world or “ecologically valid” stimuli is of particular interest for two reasons: first, such an investigation can reveal perceptual grouping processes that occur under natural conditions; second, there is growing evidence suggesting that neuronal populations behave differently under natural conditions than they do under controlled experimental conditions (Hasson et al., 2004). For instance, responses of neurons to simple, controlled stimuli are often not predictive of how they respond to more complex, natural stimuli (Touryan et al., 2005). Currently, the brain systems underlying the segmentation of ecologically valid stimuli, particularly in the auditory domain, are poorly understood.

Music is innate to all human cultures, and there is evidence suggesting that the ability to appreciate music can develop even without explicit training (Trehub, 2003); hence, music is considered an ecologically valid auditory stimulus. Like speech, music is hierarchically organized (Cooper and Meyer, 1960; Lehrdahl and Jackendoff, 1983); perceptual event boundaries in music exist at several well-defined hierarchical levels and time scales, including discrete tones, rhythmic motifs, phrases, and movements. In the Western classical tradition, the highest hierarchical level within a musical work is the *movement*, which is defined as “the primary self-contained section of a large composition” (Apel, 1969). Adjacent movements within a single work are generally delimited by a number of different cues: changes in tempo (gradual slowing), tonality (changes in the tonic or key center), rhythm, pitch, timbre, contour, and boundary silences (gradual drop in intensity). While each movement may last from several to ten or more minutes, transitions between movements take place over the time scale of a few seconds. Movement *transitions* are perceptually salient event boundaries that demarcate such long time-scale structural changes, partitioning a large-scale musical composition into

thematically coherent subsections. These coarse-grained transitions are easily perceived by musically untrained listeners (nonmusicians), unlike finer-grained transitions (such as “phrase transitions”) that occur over shorter timescales of 1 s or less, which even musically trained listeners can find difficult to perceive (Knosche et al., 2005). Here, we examine how the brain accomplishes event segmentation at coarse-grained boundaries in ecologically relevant stimuli by isolating brain responses immediately before, during, and after these musical movement transitions. Studying such segmentation processes in music may be a useful window into similar processes in other domains, such as spoken and signed language, visual perception, and tactile perception.

Literature on event segmentation of ecologically valid stimuli is scarce; no previous study, to our knowledge, has directly addressed the question of event segmentation in the auditory domain, and specifically in music. A previous study by Zacks et al. (2001) examined event segmentation using video clips of everyday activities. However, event boundaries in their stimuli were found to be subjective, highly variable, and difficult to characterize by normative criteria. On the other hand, musical event boundaries are perceptually salient and theoretically well-defined. This characteristic, taken together with its ecological validity and inherently temporal nature, makes music uniquely suited to the study of the dynamics of event segmentation of ecologically valid stimuli that unfold over time. On the one hand, we have learned a great deal from related studies that used electroencephalography (EEG) and magnetoencephalography (MEG) to investigate the perception of fine-grained temporal structure in music (Knosche et al., 2005; Maess et al., 2001; Popescu et al., 2004). These studies have suggested the involvement of a wide range of brain structures, including Broca’s area (Maess et al., 2001), motor structures (Popescu et al., 2004), and the anterior and posterior cingulate cortex (Knosche et al., 2005), in the dynamical aspects of music structure processing. However, these experiments generally use laboratory-manipulated, short musical segments as stimuli that offer the experimenters control over the stimulus parameters; the trade-off is that such stimuli tend to be musically unnatural, lack ecological validity, and are not part of the normal musical experience. For instance, Knosche et al. (2005) studied the perception of phrase structure using EEG/MEG by examining differential brain responses of musicians to phrased versus unphrased musical stimuli. The latter were created by removing the phrase boundaries and filling in pauses between phrases with notes. An MEG study by Maess et al. (2001) employed harmonically inappropriate chords inserted into a major-minor tonal context. Similarly, Popescu et al. (2004) used MEG to study the perception of rhythmic structure during music listening; they presented a single motif component lasting about 10 s. This approach allowed them to focus on the processing of a specific local musical structure, but precludes generalizability to the wide variety of musical structures typically encoun-

tered in “real” music. Finally, whereas temporal resolution with EEG/MEG is excellent, brain regions identified with EEG/MEG source localization procedures are approximate at best, and inaccurate at worst (Menon and Crotaz-Herbette, 2005). Thus, the functional neuroanatomy and dynamics of brain processes underlying the parsing and segmentation of ecologically valid musical stimuli remain largely unknown.

Here, we examine event segmentation using an experimental design employing “authentic” musical stimuli and a passive listening task that simulates real-world music listening. We used fMRI to scan 18 musically untrained participants while they listened to two 8–10 min long segments of symphonies by the English baroque composer William Boyce (1711–1779). We then attempted to uncover the neural dynamics of event segmentation of the musical stream by isolating time-dependent sequences of brain responses in a 10 s window surrounding movement transitions. Since the structural changes accompanying such transitions occur over a timescale of a few seconds, we could elucidate these dynamics with a temporal precision that was well within the resolving power of fMRI and with a spatial resolution that is generally impossible to obtain with scalp-recorded EEG or MEG. We then used latency analyses, independent component analysis (ICA), and Granger causality analysis (GCA) of the fMRI data to confirm and further explore our findings regarding the neural dynamics underlying event segmentation at movement transitions.

RESULTS

Movement Transitions Are Perceptually and Physiologically Salient Event Boundaries

Because we used a passive listening task during brain imaging, we conducted a follow-up behavioral study outside the scanner to ensure that participants could accurately perceive the movement transitions. We used the same stimuli that were used in the scanner, with the only difference being that the subjects now had to respond by pressing a button whenever they heard a transition (see [Supplemental Experimental Procedures](#) in the [Supplemental Data](#) available with this article online). They responded with different buttons for what they perceived to be large and small transitions. The behavioral data summarized in [Figure 1A](#) show that participants successfully identified over 90% of the movement transitions as points of marked structural change in the music (see [Supplemental Experimental Procedures](#) and [Table S1](#)). To examine whether the movement transitions were perceived as salient stimuli during the passive listening task inside the scanner, we examined changes in autonomic nervous system reactivity using cardiovascular signals that were acquired simultaneously with the brain imaging data. We found a significant increase in the variability of the interval between consecutive R waves (RR variability) during the movement transition compared to the baseline ([Figure S4](#)). These results indicate that movement

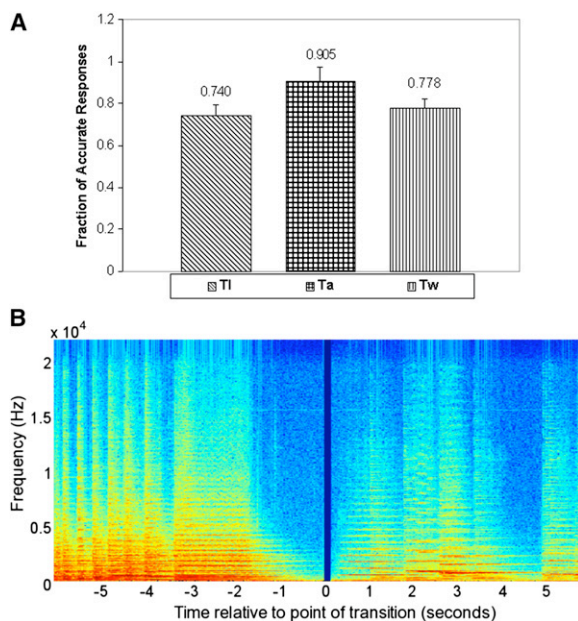


Figure 1. Behavioral Responses and Spectrogram of Stimulus during the Transition

(A) Behavioral data revealed that study participants demonstrated a high level of accuracy and uniformity in identifying movement transitions when these occurred in the stimulus. Hence, movement transitions are easily and unambiguously perceived even by musically untrained listeners. T_l is the fraction of movement transitions correctly identified as large transitions; T_a is the fraction of movement transitions correctly identified as large or small transitions; and T_w is the number of movement transitions within the observation window expressed as a fraction of the total number of large transitions indicated by the participants. Error bars denote standard error of the mean (SEM) across subjects.

(B) Spectrogram of the stimulus plotted in a 10 s window surrounding a representative movement transition (corresponding to the transition heard in the audio track of [Movie S1](#)). The dark vertical line in the spectrogram, representing the minimum of the stimulus amplitude envelope, corresponds to the “point of transition.” The x axis represents time relative to the point of transition (in seconds), with negative time denoting time before the point of transition. The “transition” itself is an extended (approximately 10 s wide) time window surrounding the “point of transition.” A transition is not a sudden point event; it is characterized by a gradual slowing down of the previous movement, followed by a brief silence, and the onset of the next movement.

transitions were perceived as salient event boundaries even by musically untrained listeners.

Time Course of Brain Responses during the Movement Transition

A movement transition in music is not a sudden “point” event; it is characterized by a gradual slowing down of the previous movement followed by a brief silence and the onset of the next movement. [Figure 1B](#) shows the spectrogram of the stimulus plotted in a 10 s window surrounding a representative movement transition; this spectrogram corresponds to the transition heard in the audio track of [Movie S1](#). We operationally defined the “point of

transition” ($t = 0$ s) as the point at which the amplitude envelope shows a marked minimum (with full knowledge that other cues not visible in the amplitude envelope could contribute to the perception of a transition). In [Figure 1B](#) this is represented by a dark vertical line in the spectrogram. We analyzed data with respect to this reference transition point (see also [Experimental Procedures](#)).

We examined the time course of activation in a 10 s window surrounding the point of transition, averaged over all movement transitions. Analysis of the data was performed with a time-shifted regressor over all transitions (to average out transition-specific effects) using the general linear model (see [Experimental Procedures](#)). The analysis revealed a strikingly right-lateralized pattern of brain responses that peaked at the point of the movement transition and diminished progressively afterward (activations contrasted against the baseline response to the rest of the music, [Figures 2A](#) and [2B](#)). Interestingly, the brief period of silence between movements meant that the activations peaked at a time when there was, in fact, little or no physical stimulus (see [Movie S1](#)).

Evidence for Right-Lateralized, Dissociable Ventral and Dorsal Networks

We detected activity in two distinct networks of brain regions at the transitions ([Figure 2](#) and [Table S2](#)): (1) a ventral fronto-temporal network, including the ventrolateral prefrontal cortex (VLPFC, BA 47, 44/45) and posterior temporal cortex (PTC, BA 21/22), which was active during the *early* part of each transition; and (2) a dorsal fronto-parietal network, including the dorsolateral prefrontal cortex (DLPFC, BA 9) and posterior parietal cortex (PPC, BA 40), which was active during the *later* part of the transition. A region-of-interest (ROI) analysis on these four regions (VLPFC, PTC, DLPFC, and PPC) confirmed that the pattern of activation during the transition was predominantly right-lateralized—all four ROIs demonstrated a significantly higher percentage of active voxels in the right compared to the left hemisphere (Wilcoxon signed-rank test; [Figure 4A](#)).

Latency and ROI Analyses Reveal that Ventral Network Activity Precedes Dorsal Network Activity

In order to validate and extend our findings of temporal changes, we conducted additional ROI and latency analyses of the BOLD responses in these regions. First, we examined latency differences in the peak of the BOLD response across brain regions using the analysis method developed by [Henson et al. \(2002\)](#). Briefly, this method provides a way to estimate the peak latency of the BOLD response at each voxel using the ratio of the derivative to canonical parameter estimates (see [Experimental Procedures](#) for details). The results of the latency analysis are shown in [Figure 3](#). The right VLPFC and PTC showed a negative latency relative to the canonical response, indicating activity in these regions during the early part of the transition, whereas the right DLPFC and PPC exhibited a positive latency relative to the canonical response,

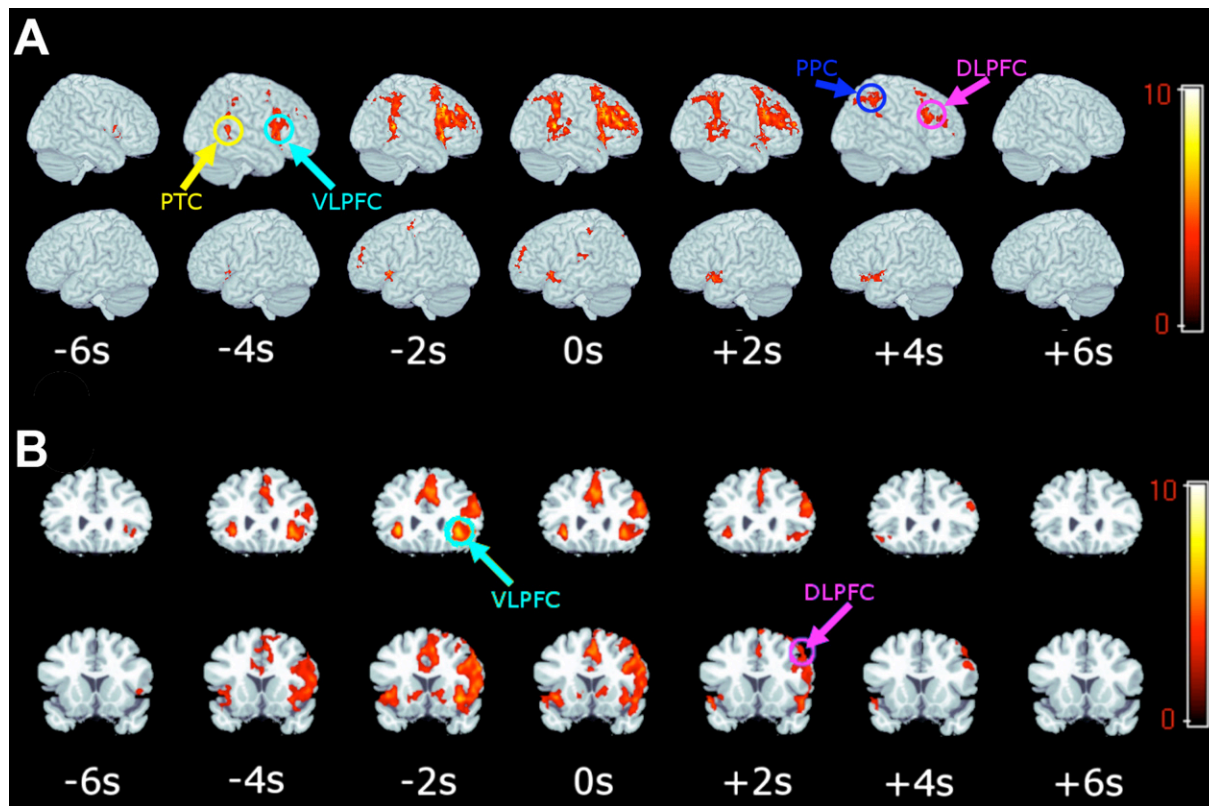


Figure 2. Temporal Dynamics of Brain Activity in a 12 s Window Surrounding the Point of the Movement Transition

(A) Surface rendering showing right (top row) and left (bottom row) hemispheric responses as a function of time (from 6 s before the point of transition to 6 s after the point of transition). Brain responses throughout the movement transition were predominantly right-lateralized. With time, activity shifted along a ventral-dorsal axis, with the ventral network—ventrolateral prefrontal cortex (VLPFC, cyan arrow) and posterior temporal cortex (PTC, yellow arrow)—active during the early part of the transition and the dorsal network—dorsolateral prefrontal cortex (DLPFC, magenta arrow) and posterior parietal cortex (PPC, blue arrow)—active during the later part of the transition.

(B) Coronal sections showing anterior ($y = +27$ mm, top row) and posterior ($y = +16$ mm, bottom row) slices through the frontal lobes. The right VLPFC, marked with a cyan arrow at $t = -2$ s, was significantly active earlier in the transition, whereas the right DLPFC, marked with a magenta arrow at $t = +2$ s, showed sustained activation later in the transition.

indicating significant activity later in the transition. Thus, this analysis provided confirmatory evidence for a pattern of brain dynamics identical to the one noted above, indicating initial activation of the ventral network followed by activation of the dorsal network (see Figure 2).

Next, the right hemispheric ROIs were analyzed to test for differential peak activity, as gauged by the maximum percentage signal change (MPSC), before, during, and after the point of transition. Figure 4B quantifies the MPSC in these ROIs one frame before ($t = -2$ s), during ($t = 0$ s), and after ($t = +2$ s) the point of transition. While the right VLPFC showed significantly higher MPSC before and during versus after the point of transition (Wilcoxon signed-rank test, $T_{17} = 14$, $p = 0.0031$), right DLPFC and right PPC exhibited higher MPSCs during and after versus before the point of transition (Wilcoxon signed-rank test; DLPFC: $T_{17} = 28$, $p = 0.0217$; PPC: $T_{17} = 35$, $p = 0.0495$). The MPSC in the PTC did not show a significant difference in activity pre- versus posttransition. Thus, ROI analysis provided further

evidence for early activation of the ventral network relative to the dorsal network during the transition.

Finally, we computed the normalized event-related BOLD response from these ROIs averaged across events and subjects (Figure 5A), raw event-related BOLD responses averaged across subjects were normalized on a 0–1 scale to facilitate comparison of the peak latency across BOLD responses with differing peak magnitudes. Time $t = 0$ s on the x axis corresponds to the point of transition. As is apparent from the event-averaged response, the peak of the BOLD response in the VLPFC and PTC occurred earlier than that of the PPC and DLPFC, and the latter had comparable peak latencies. These observations demonstrate that the peak response of the ventral network areas precedes that of the dorsal network areas during the segmentation of movement transitions.

While these analyses provided clear evidence for latency differences in the peaks of the BOLD responses between the ventral and dorsal networks, a precise

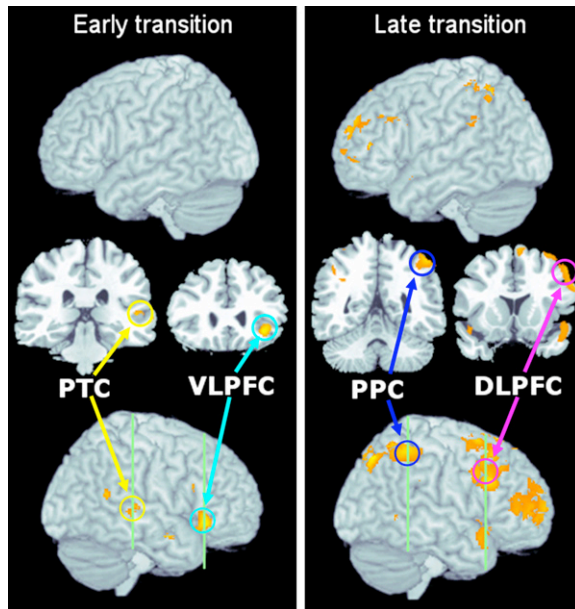


Figure 3. Latency Analysis Reveals Earlier Activity in the Ventral Compared to the Dorsal Network during the Transition

Latency analysis (Henson et al., 2002) of the fMRI signal revealed negative latency in the ventral network (VLPFC and PTC) relative to the canonical response, and a positive latency in the dorsal network (DLPFC and PPC). Thus, peak activity in the ventral network occurred earlier in the transition and that of the dorsal network occurred later in the transition. Surface rendering of left and right hemisphere responses (top and bottom rows); coronal sections at $y = +27$ mm (VLPFC), -30 mm (PTC), $+16$ mm (DLPFC), and $+49$ mm (PPC) are shown in the middle row.

quantification of the latencies using the Henson et al. (2002) approach is not possible due to high estimation errors in the derivative to canonical ratio. In order to provide a means of quantifying the differences in latencies of activation between these ROIs, we attempted to compute the onset latency of the BOLD response. Briefly, the onset latency of the BOLD response is defined as the point of inflection of the response from its baseline value; it may be used as a measure of the onset latencies of the underlying neural activity (Formisano and Goebel, 2003; Menon et al., 1998). In order to compute the onset latencies, we followed the method of Sterzer and Kleinschmidt (2007), using a Fourier model to fit the event-related BOLD response; this method avoids a priori assumptions about the shape of the response (for details on the calculation of onset latencies, see Supplemental Data). The results of this analysis (indicated in Figure 5B and Figure S1) revealed that the onset of the BOLD response in the VLPFC, in the ventral network, preceded the DLPFC, in the dorsal network, by 2.10 ± 0.75 s (mean \pm SE, $p = 0.0179$, $T_{17} = 26.5$, Wilcoxon signed-rank test) and the PPC, in the dorsal network by 1.42 ± 0.45 s (mean \pm SE, $p = 0.0032$, $T_{17} = 11$, Wilcoxon signed-rank test). Mean onset latency of the PTC was greater than that of the VLPFC, but less than that

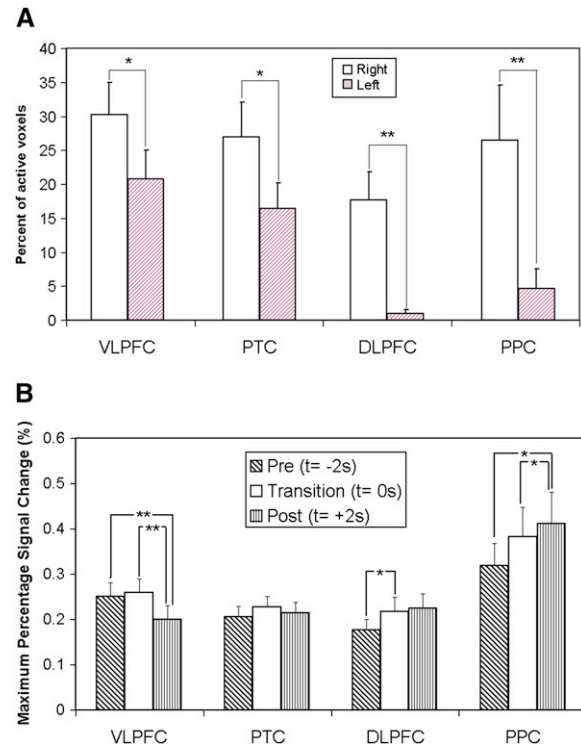


Figure 4. Hemispheric and Regional Differences in Brain Activity during the Movement Transition

(A) Right- (unshaded bars) and left- (shaded bars) hemisphere responses in the VLPFC, PTC, DLPFC, and PPC during event segmentation. All four regions showed significantly greater activation in the right hemisphere (either at the $p < 0.01$ level [*] or the $p < 0.05$ level [†]; Wilcoxon signed-rank test; error bars denote SEM across subjects). (B) Maximum percentage signal change in the ROIs before (pre, diagonally hatched bars), during (bars with no hatching), and after (post, vertically hatched bars) the point of transition. Plotting the maximum percentage signal change (MPSC) in the ROIs across the transition revealed that the VLPFC had significantly higher BOLD signal before and during versus after the point of transition. The DLPFC and PPC revealed the opposite trend, with greater signal during and after versus before the point of transition (either at the $p < 0.01$ level [**] or the $p < 0.05$ level [†]; error bars denote SEM across subjects).

of the dorsal network regions (DLPFC and PPC) (Figure 5B); however, these other latency differences did not reach significance (at the $p < 0.05$ level). Information flow between networks of neurons occurs over the timescale of several tens to hundreds of milliseconds; hence, the exact values of the latency differences reported here may not directly represent neural latency differences between these ROIs. However, onset latency differences provide a faithful measure of the relative differences in latency of onset of the underlying neural activity (Formisano and Goebel, 2003; Henson et al., 2002; Menon et al., 1998; Sterzer and Kleinschmidt, 2007; see also control analyses in Supplemental Data). In our case, these point to a clear order in the activation of prefrontal cortical (PFC) regions during the movement transition—the ventral network (VLPFC) activation followed by the dorsal network (DLPFC).

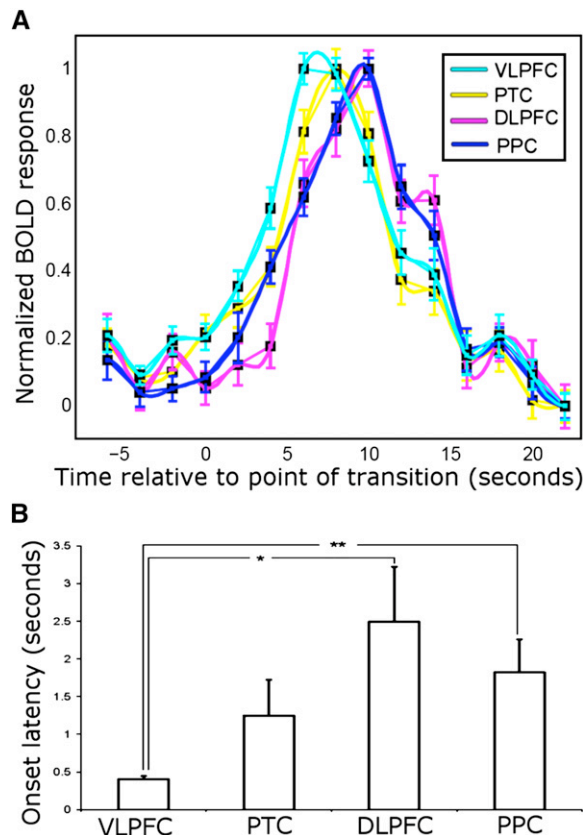


Figure 5. Peak and Onset Latency Differences in the Ventral and Dorsal Networks

(A) Normalized event-related BOLD responses from the VLPFC, PTC, DLPFC, and PPC. Raw BOLD responses were normalized to their peak value. The peak of the BOLD response in the ventral network (VLPFC, cyan; PTC, yellow) occurred earlier than the dorsal network (DLPFC, magenta; PPC, blue). The BOLD response is spline interpolated (thick curve) for demonstration purposes. Thin lines of the same color connecting successive points in the BOLD response are also shown for reference. Error bars correspond to SEM across subjects.

(B) Onset latencies of event-related responses in the VLPFC, PTC, DLPFC, and PPC. The VLPFC showed the earliest onset, followed by the PTC, PPC, and the DLPFC. VLPFC onset was significantly earlier than the DLPFC (2.10 ± 0.75 s, $p < 0.05$) and the PPC (1.42 ± 0.45 s, $p < 0.01$). Other onsets did not show significant differences. Error bars denote SEM across subjects.

Granger Causality Analysis of Ventral and Dorsal Brain Regions

Finally, we hypothesized that if the observed pattern of latency differences truly reflects the underlying dynamics of activation, ventral regions, notably the VLPFC, may exert causal, or directed, influences on the regions in the dorsal network. To test this hypothesis, we used Granger causality analysis (GCA), a technique that has been successfully used to measure directionality of signaling in cortical networks based on the temporal history of BOLD signal changes (Miller and D’Esposito, 2005; Roebroek et al., 2005). Briefly, activity in brain region A is said to “Granger

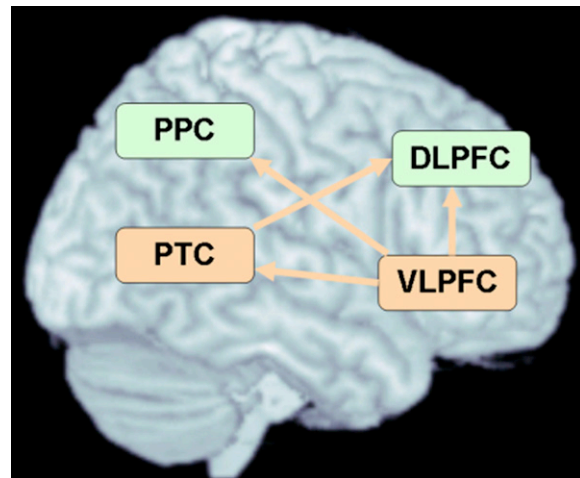


Figure 6. Granger Causality Analysis Reveals Predominance of Causal Connections from Ventral to Dorsal Network

Granger causality analysis (GCA) of time series from individual regions in the right ventral fronto-temporal network (red regions) and dorsal-frontoparietal network (green regions). Arrows indicate significant causal connections from the ventral network regions to dorsal network regions ($p < 0.05$). GCA showed a predominance of causal influences from the VLPFC and PTC to the DLPFC and PPC, indicating a causal, directional influence from the ventral to the dorsal network. Particularly, activity in the right VLPFC “Granger caused” all of the other ROIs, implicating the VLPFC as the key modulator of brain dynamics induced by the movement transition.

cause” activity in brain region B if A’s time series proves useful in predicting B’s future time series (Roebroek et al., 2005). GCA was performed on the BOLD time series extracted from the VLPFC, PTC, PPC, and DLPFC separately for each subject (see Experimental Procedures). Confirming our hypothesis, GCA (across subjects) revealed a predominance of connections from the ventral to the dorsal network (Figure 6, all connections significant at the $p < 0.05$ level, Wilcoxon signed-rank test). Specifically, the right VLPFC activation was causal to the activation in the PTC, DLPFC, and PPC, and the right PTC activation was causal to activation in the DLPFC, indicating consistent causal influences from the ventral to the dorsal network.

Converging Evidence for Distinct Ventral and Dorsal Networks Using ICA

Converging evidence for distinct functional networks subserving event segmentation in music was also obtained from an independent component analysis (ICA) of the data. ICA is a model-free analysis technique that incorporates no a priori hypothesis on the temporal course of the brain response. It yields spatially independent components, each with an associated time course (Beckmann and Smith, 2004). Random-effects analysis of ICA components clustered by spatio-temporal similarity across subjects (see Supplemental Experimental Procedures) revealed activation of two distinct right-lateralized functional networks—the ventral fronto-temporal network and the

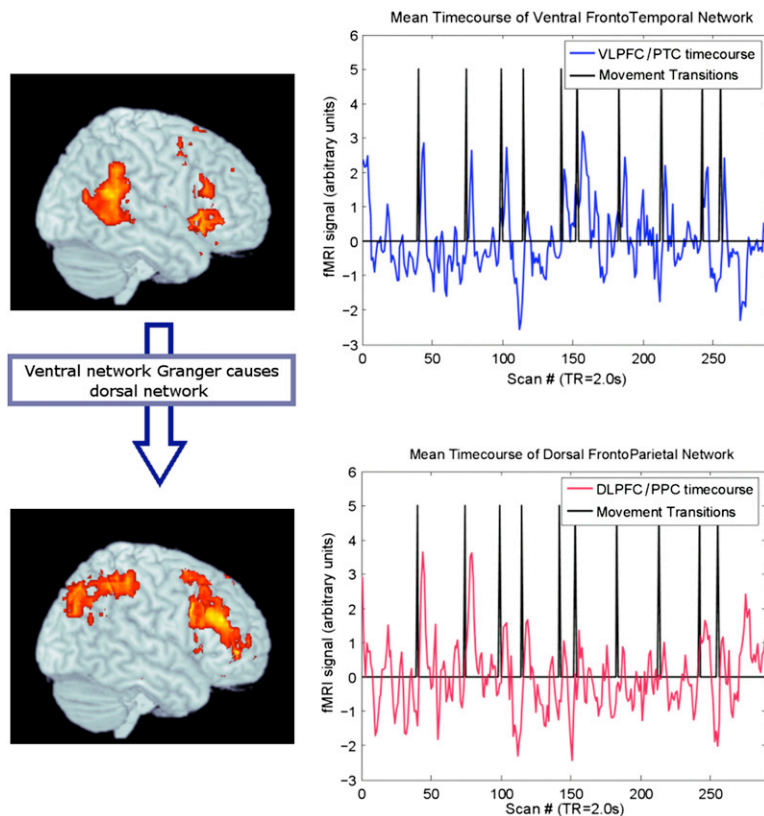


Figure 7. Converging Evidence for Dissociable Ventral and Dorsal Functional Networks at the Movement Transition Revealed by ICA

Independent component analysis (ICA) provided converging evidence for dissociable ventral fronto-temporal (top left panel) and dorsal fronto-parietal networks (bottom left panel). The right panels show the subject averaged time courses of the ventral network (top right panel, in blue) and the dorsal network (bottom right panel, in red). The component time courses tracked the movement transitions (shown as black event markers, top and bottom graphs in the right panel) with striking consistency even though no *a priori* model of the transitions had been specified in the analysis. Confirming the pattern observed with regional time courses (Figure 6), Granger causal analysis of the time courses of the two independent components revealed a causal link from the ventral to the dorsal network.

dorsal fronto-parietal network (left panel, Figure 7). Interestingly, the mean time course of the group components averaged across subjects (right panel, Figure 7) tracked the transitions (black vertical bars) with striking consistency even though *no a priori model* of the transitions had been specified in the analysis. GCA on the ICA-derived time courses revealed that the ventral network activity led, or “Granger caused,” the dorsal network activity. These results obtained from the entirely different perspective of model-free analysis provide strong corroborative evidence for a functional dissociation between the ventral and dorsal networks involved in event segmentation of music.

Potential Confounds: Amplitude Variation, Physiological Changes, and Oddball Effects

Movement transitions are typically accompanied by marked changes in sound amplitude. To rule out the possibility that the brain responses at the movement transitions merely reflect tracking of the increases or decreases in overall amplitude, we performed further analyses to identify those brain regions that respond only to fluctuations in the amplitude envelope of the stimuli (see [Supplemental Experimental Procedures](#) for details). As shown in [Figure S2](#), only activity in the bilateral auditory cortices along the mid- and posterior superior temporal gyrus was positively correlated with amplitude. Further, no brain regions showed negative correlations with amplitude.

These results suggest that brain responses observed during the movement transitions are not due to changes in sound amplitude per se. Next, in order to test whether physiological changes at the transition were chiefly responsible for the observed brain activations, we identified brain regions responding to changes in the RR variability (see [Supplemental Data](#)). Only the anterior cingulate cortex and bilateral anterior insula tracked changes in RR variability that occurred during the movement transitions (data not shown).

One further concern that we addressed was whether brain activations observed during the movement transition reflect “oddball” effects that arise from unexpected stimulus occurrence ([Crottaz-Herbet and Menon, 2006](#)). The movement transitions in the stimuli used in our study occur, on the average, once every 60 s, but unlike standard oddball stimuli, they are not unexpected—they are characterized by a gradual slowing down of the music, a brief pause, followed, often, by a gradual increase in stimulus amplitude. Nevertheless, in order to provide conclusive evidence, we used a random-effects analysis to directly compare activation during the movement transition with brain responses elicited by auditory oddball stimuli ([Crottaz-Herbet, and Menon, 2006](#); see [Supplemental Experimental Procedures](#)). While a few regions (such as the PTC, cerebellum, and cingulate cortex) showed overlap between the two tasks, the oddball task did not recruit the extensive dorsal and ventral network activations

observed during passive segmentation in the present study (Figure S3). Furthermore, brain responses to movement transitions, contrasted with oddball responses, revealed significant responses in all the regions identified originally (Figure S3, bottom panel, and Table S4). These findings indicate that brain processes engaged during the perception of the movement transitions are distinct from those elicited by the oddball task.

One potential confound while performing chronometric analysis on the BOLD response is the possibility that the observed effects reflect vascular rather than neural dynamics. As seen in Figure 3, only the right hemispheric regions showed significant differences in the patterns of early versus late latency of responses when the data were analyzed using the voxel-based approach of Henson et al. (2002); no such effects were detected in the corresponding left hemispheric regions. This suggests that the latency effects that we observed were neural, rather than vascular, in origin. In order to further validate the relatively novel onset latency and Granger causal analyses used in our study, we carried out the following additional control studies: (1) we used an entirely different approach for the estimation of onset latencies (Menon et al., 1998); we expected to observe a pattern of results similar to ones shown in Figure 5B; (2) we used a different fMRI dataset (Steinberg working memory paradigm, Chang et al., 2007) wherein the visual encoding phase precedes the motor response phase; we predicted that our methods of onset latency should discover earlier onset in the visual areas compared to the motor areas; and (3) we performed GCA on the Steinberg data set where we expected to see a causal influence from the visual cortex to the motor cortex. Our findings exactly matched our predictions in each case (Figures S5 and S6), thereby improving confidence in our findings and providing support for the view that the effects reported reflect underlying neural, rather than vascular, processes (for details see Supplemental Data).

DISCUSSION

In this study, we attempted to characterize the neural dynamics of event segmentation in music. We analyzed brain responses during the parsing of movement transitions, event boundaries at one of the highest levels of structural hierarchy in music. We used a passive listening task that maintained the ecological validity of the listening experience. Moreover, despite the passive nature of the task, several lines of evidence from our study suggest that movement transitions, rather than being merely perceived as pauses, are an important component of the natural music listening experience (see Supplemental Discussion for a more detailed perspective on these issues). Importantly, our study provides converging evidence, from both model-dependent and model-free analyses of event-related responses, for dynamic brain changes underlying musical event segmentation during natural listening conditions.

Auditory Scene Analysis under Natural Listening Conditions

Our finding of distinct dorsal and ventral networks in event segmentation represents an important step toward understanding auditory scene analysis under natural listening conditions and significantly expands on our current knowledge of event segmentation processes in the brain. Event boundaries in our study are well defined from a music-theoretical perspective and were consistently identified at both the behavioral and psychophysiological levels. We found a pattern of brain responses that were maximal at the event boundaries when, paradoxically, no stimulus was present. Our analysis of the temporal dynamics across the movement transition uncovered two distinct functional networks that are triggered at different times during the transition: a ventral fronto-temporal network (VLPFC and PTC) that onsets earlier in the transition, followed in time by a dorsal fronto-parietal network (DLPFC and PPC). Both of these networks are significantly right-lateralized, as shown in Figure 2A. Although the right hemisphere has been implicated in music processing (Brown et al., 2004; Zatorre et al., 1993), its precise role in music perception remains poorly understood, and lateralization of activation for music processing has never been adequately tested. Our findings suggest that the right hemisphere plays a dominant role in the perceptual segmentation of salient, coarse-grained event boundaries in music.

Our findings of segregated ventral and dorsal functional networks are consistent with recent anatomical studies of brain connectivity in both monkeys and humans. Anatomical tracer studies in nonhuman primates have identified a “what” pathway connecting the rostral auditory belt areas (anterolateral or AL region) to the ventral prefrontal frontal cortex (areas 12 and 45) and a “where” pathway that connects the caudal belt areas (caudolateral or CL region) to the dorsolateral prefrontal cortex (areas 46 and 8a) (Romanski et al., 1999; Kaas and Hackett, 2000). Similarly, diffusion tensor tractography in humans has revealed white matter connections between the PTC (BA 21/22 and 37) and the VLPFC (BA 47 and 45) (Barrick et al., 2007). These observations suggest that direct anatomical connections may mediate the tight functional coupling observed in the ventral and dorsal networks and further suggest that such tight coupling may impose hierarchical constraints on information processing in these networks (Mesulam, 1990). However, the dorsal-ventral networks identified in our study differ from the “classic” auditory what-where pathways in two important respects, one structural and the other functional. While there is some overlap between the what-where pathways and our dorsal-ventral networks, the two are not identical: whereas the prefrontal cortex nodes in the dorsal-ventral networks correspond to the ventral and dorsal prefrontal cortex nodes of the what-where pathway, there is little correspondence between the two in PTC and the PPC. Functionally, both the dorsal and ventral networks become active during event segmentation, and, therefore, they cannot be conflated with the putative what-where pathways.

Rather, the dorsal-ventral networks show striking overlap with the brain regions identified during visuo-spatial attention tasks (Corbetta and Shulman, 2002).

The Role of the Ventral and Dorsal Networks in Event Segmentation

Prediction and anticipation are truly at the heart of the musical experience. Even nonmusicians are actively engaged, at least subconsciously, in tracking the ongoing development of a musical piece and forming predictions about what will come next. Typically in music, *when* something will come next is known, due to music's underlying pulse or rhythm (what musicians call the "tactus"), but what is less known is *what* will occur next. There is an important link between such predictive processes and the formation of event boundaries: in music, the VLPFC has been consistently implicated in the detection of violations in musical expectancies or predictions (such as violations in chord and harmonic expectancies) even in musically untrained listeners (Koelsch et al., 2002; Maess et al., 2001; Tillmann et al., 2006). Extant literature supports the idea that the ventral network detects a mismatch between ongoing expectation and sensory events (Macaluso et al., 2002; Astafiev et al., 2006). The mismatch between ongoing expectation and sensory input may be one factor that induces event segmentation: event boundaries are typically perceived when transient errors in predictions arise (Zacks et al., 2007). For instance, when a harmonic context is followed by an unrelated/unexpected chord (Maess et al., 2001), the deviant chord needs to be grouped into a separate entity from the preceding context, thereby requiring the formation of a segmentation boundary at the point of violation of harmonic expectation. Thus, predictive processes and violations in expectancies represent two important ways in which segmentation boundaries are constructed in music. Our findings suggest that the ventral network plays an important role in this segmentation process.

On the other hand, a wide range of neuroimaging and neurophysiological studies have demonstrated coactivation of the DLPFC and PPC in the dorsal network during top-down signaling for feature or object attention (for a review, see Corbetta and Shulman, 2002) and during manipulation/monitoring of information in working memory (Fletcher and Henson, 2001; Petrides, 2005). Our results suggest that these regions form a tightly coupled network that plays an important role in directing and maintaining attention during the movement transitions and in the perceptual updating that ensues. The DLPFC (BA 9) has been specifically implicated in such perceptual updating of events in working memory even in the absence of behavioral responses and explicit cognitive control (Wager and Smith, 2003).

Converging Evidence for Dissociable Ventral and Dorsal Networks

Although several other studies have reported dissociable activations in dorsal and ventral brain regions (Macaluso

et al., 2002; Shulman et al., 2003; Burgund et al., 2005; Astafiev et al., 2006; Dosenbach et al., 2006), our finding indicate that these regions are tightly coupled and that they form distinct, statistically independent *networks*. Evidence for the presence of two independent networks comes from ICA analysis of the four-dimensional fMRI data. This analysis does not make any assumptions about the time course of event-related responses and instead attempts to derive statistically independent spatial patterns of brain responses (Beckmann and Smith, 2004). Our analysis clearly showed that the ventral and dorsal regions identified in the event-related analysis above segregate into two independent components whose time courses accurately track the transitions. One component includes the VLPFC and the PTC, and the other includes the DLPFC and the PPC. GCA on the ICA components also revealed a statistically significant causal link directed from the ventral network to the dorsal network across subjects, indicating that these networks are tightly coupled during event segmentation.

Based on a synthesis of findings from a wide range of animal electrophysiology and human imaging experiments, Corbetta and Shulman (2002) have hypothesized segregation of similar ventral fronto-temporo-parietal and dorsal fronto-parietal regions in visuo-spatial attention. They propose that right-lateralized ventral fronto-temporo-parietal regions are involved in the detection of salient stimuli, and bilateral dorsal fronto-parietal regions are involved in attentional signaling for feature or object detection in visual stimuli. A comparison of their dorsal and ventral regions (Figure 7a in Corbetta and Shulman, 2002) with those discovered by our analysis (Figure 7 of the present article) reveals a remarkable overlap in the foci of activation. Direct experimental evidence for the recruitment of these distinct regions as functionally coupled and causally linked *networks* in perceptual tasks has, however, thus far been lacking. Our findings not only provide fresh support for this hypothesis but also characterize the dynamical relations between ventral and dorsal networks in the processing of ecologically relevant stimuli. Further, our findings indicate that the ventral network is right-lateralized not only for orienting attention to visual stimuli but also during segmentation of salient auditory events. These results suggest that neither of these networks is specific to visual processing and may, in fact, correspond to polymodal association areas involved in the processing of salient, temporally structured sensory stimuli.

In order to further examine the interactions of these networks, we used Granger causality analysis on fMRI time series extracted from four dorsal and ventral regions (Figure 6). Unlike models of effective connectivity that describe the strength of interaction between cortical regions (Friston, 1994), GCA provides a robust way to assess the directionality of causal interactions (Seth, 2005; Roebroeck et al., 2005; Lungarella et al., 2007). ROI-based GCA revealed that ventral network activity "Granger caused" activity in the dorsal network regions; specifically, the VLPFC Granger-caused responses in all of the

other ROIs, thereby implicating the VLPFC as a key modulator of the brain dynamics that occur during the movement transition. These findings provide evidence for a critical and causal role of the VLPFC in detecting and updating brain responses to event boundaries.

A Putative Model for Event Segmentation of Ecologically Valid Stimuli

Synthesizing our results with previous observations from the literature (Corbetta and Shulman, 2002; Levitin and Menon, 2003), it is possible to construct a tentative, yet informative picture of information processing involving temporally structured, ecologically valid stimuli in the brain: the ventral fronto-temporal network appears to be involved in the detection of salient events based on the sensory features of the stimulus stream—this network essentially signals the occurrence of a salient event boundary in the stimulus. The dorsal fronto-parietal network then turns the spotlight of attention to the event boundary and, upon commencement of the next event, presumably performs a perceptual update of the transition in working memory. Causal connections from the ventral fronto-temporal network to the dorsal fronto-parietal network indicate that the saliency detection network could indeed act as a “circuit breaker” for the dorsal network, as hypothesized by Corbetta and Shulman (2002). Thus, the ventral network directs attention to salient event boundaries during segmentation of the sensory stream, thereby aiding the detection of objects or features in the sensory stream. In our study, these dynamic changes reflect the brain’s evolving responses to different phases of event segmentation during the movement transition characterized by the termination of one movement, a brief pause, followed by the initiation of a new movement and the perceptual updating that ensues.

Future Directions

Future work should further explore auditory event segmentation using stimuli that are carefully manipulated to retain ecological relevance, while at the same time dissociating component processes such as saliency detection, direction of attention, and perceptual updating in working memory. Further studies are also needed to understand how the ventral and dorsal networks identified here are placed relative to the putative “what” versus “where” pathways that are thought to play an important role in auditory processing (Arnott et al., 2004; Zatorre et al., 2002). Our study has addressed the question of event segmentation at one important level of the hierarchy of event boundaries: at the level of the movement transition. Further studies are also needed to examine the dynamics of event segmentation at finer-grained event boundaries in the musical hierarchy, such as phrase boundaries. However, unlike the movement transitions studied here, such boundaries are likely to be less salient, more subjective, and not uniformly detected by musically naive listeners, as even musically trained listeners have difficulty in clearly perceiving these finer-grained transitions (Knosche et al., 2005). Moreover,

the dynamics of phrase segmentation, for example, occurs much more rapidly and are unlikely to be resolved with the temporal resolution of fMRI alone. A goal for the near future is to combine the EEG and fMRI methods to elucidate the fast spatio-temporal dynamics underlying event segmentation of fine-scale event boundaries. Investigation of the hierarchical temporal and spatial organization of auditory information processing in terms of phase resetting of intrinsic brain rhythms across the frequency spectrum from slow to fast oscillations (Lakatos et al., 2007, 2005; Canolty et al., 2006) remains a significant challenge.

EXPERIMENTAL PROCEDURES

Participants and Stimuli

Eighteen right-handed participants (eight females), ages ranging from 19 to 27 years, with little or no musical training (as in Maess et al., 2001) participated in the experiment. The stimuli consisted of digitized sound files (22,050 Hz sampling rate, 16 bit mono) comprising the eight symphonies of English late-baroque period composer William Boyce. These symphonies were chosen because they are relatively short and comprise several well-defined movements. The eight symphonies were divided up into two runs of four symphonies each, each run lasting about 9 min. The symphonies contain 20 movement transitions (events of interest here), which provided a sufficient number of events for an event-related fMRI analysis. Participants were instructed to passively listen to the musical stimuli. The task was programmed with E-Prime (PSTNET, Pittsburgh, PA; www.pstnet.com), and stimuli were presented binaurally over noise-reducing headphones using a custom-built magnet-compatible system at a sound level comfortable to the participants.

Event Structure of the Movement Transitions

We find it relevant to mention here a subtle distinction in terminology used in the analyses. We use the term “point of transition” to refer to the scan frame immediately following the offset of the preceding movement (a point in time); typically, this point corresponds to a brief period of silence between the movements. In Figure 1B, the point of transition is represented by the dark vertical line in the spectrogram at $t = 0$ s. All of the figures (Figure 1B, Figure 2, Figure 4B, and Figure 5A) are plotted with the point of transition corresponding to zero time ($t = 0$). On the other hand, unqualified use of the word “transition” refers to an extended (approximately 10 s wide) time window surrounding the point of transition. For instance, Figure 1B shows the spectrogram of the stimulus plotted in a 10 s window surrounding a representative point of transition (movement transition); this spectrogram corresponds to the transition heard in the audio track of Movie S1.

fMRI Data Acquisition

fMRI acquisition followed a procedure similar to that described in Levitin and Menon (2003), and details are provided in the Supplemental Data.

fMRI Data Analysis

fMRI data were preprocessed using SPM2 (<http://www.fil.ion.ucl.ac.uk/spm>). Functional volumes were corrected for movement-related effects (Friston et al., 1996), spatially normalized to stereotaxic Talairach coordinates, resampled every 2 mm using sinc interpolation, and smoothed with a 4 mm Gaussian kernel to reduce spatial noise. One subject was excluded from the fMRI analysis due to considerable artifacts in the data. Statistical analysis was performed using the general linear model (GLM) and the theory of Gaussian random fields as implemented in SPM2. A within-subjects procedure was used to model all the effects of interest for each subject. A regressor for modeling the effects of interest was created by convolving the hemodynamic

response function with an impulse function that peaked at each movement transition. Confounding effects of fluctuations in global mean were removed by proportional scaling where, for each time point, each voxel was scaled by the global mean at that time point. Although global scaling is not necessary for most fMRI studies, in the present case it is important to incorporate this additional step because we are interested in event-related brain responses over and beyond global brain responses to the constant auditory stream (Macey et al., 2004). Low-frequency noise was removed with a high-pass filter (0.5 cycles/min) applied to the fMRI time series at each voxel. Effects of interest for each subject were then defined with the relevant contrasts of the parameter estimates. Group analysis was performed using a random-effects model that incorporated a two-stage hierarchical procedure. In the first stage, contrast images for each subject and each effect of interest were generated as described above. In the second stage, these contrast images were analyzed using a general linear model to determine voxel-wise *t* statistics. Finally, the *t* statistics were normalized to *Z* scores, and significant clusters of activation were determined using the joint expected probability distribution of height and extent of *Z* scores (Poline et al., 1997), with height ($Z > 2.33$; $p < 0.01$) and extent thresholds ($p < 0.05$). Maxima and all coordinates are reported in MNI coordinates. Activations were overlaid on a structural Talairach template image using MRICro (<http://www.sph.sc.edu/comd/rorden/mricro.html>).

ROI Analysis

ROI analysis was performed using the Marsbar software package (<http://marsbar.sourceforge.net>). Percentage of active voxels was calculated from predefined anatomical ROIs (from the AAL atlas) as the percentage of voxels that crossed the $Z = 2.33$ score threshold (corresponding to $p < 0.01$). Spherical ROIs were then defined as the set of voxels contained in 6–10 mm spheres centered on the peaks of activation clusters obtained from the GLM analysis. ROI centers and radii were defined as follows: VLPPFC, 10 mm radius sphere centered at [36 28 -6] mm; PTC, 10 mm sphere centered at [57 -45 9] mm; DLPFC, 8 mm sphere centered at [45 16 45] mm; and PPC, 6 mm sphere centered at [54 -50 50] mm. The mean time course in each ROI was extracted by averaging the time courses of all of the voxels (in the preprocessed data) contained in the ROI. The maximum percentage signal change was then calculated one frame before, during, and one frame after the movement transition and averaged over sessions for each subject (Figure 4B).

Latency Analysis

The latency of the BOLD response relative to the canonical response at each voxel was estimated by the ratio of the derivative to canonical parameter estimates (according to Henson et al., 2002) obtained from the original SPM analysis. The response latency map was created by transforming the derivative to canonical ratio for each voxel with a sigmoidal logistic function parameterized by two constants, *C* and *D*. As this was a first-pass analysis to estimate latency responses, we chose the values of *C* and *D* to be 1.78 and 3.10, respectively (Henson et al., 2002). A statistical parametric map (SPM) of BOLD latency was then created by entering the individual subject latency images (smoothed with an 8 mm FWHM isotropic Gaussian kernel) into a second-level random-effects analysis. Group-level latency SPMs were masked with voxels that survived the $p < 0.05$ (corrected) level in the *F* tests in the original SPMs. Group maps were height thresholded at $p < 0.025$ uncorrected (as in Henson et al., 2002), and only regions comprising at least ten contiguous voxels are reported.

Granger Causal Analysis

GCA was performed using the Causal Connectivity Analysis Toolbox (Seth, 2005), with modifications based on the methods proposed by Roebroeck et al. (2005). First, the mean time course from each ROI was extracted for all subjects. This time course was then high-pass filtered at 0.5 cycles per minute. GCA was performed to test for causal

influences between ROIs taken pairwise. A difference of influence term ($F_{x \rightarrow y} - F_{y \rightarrow x}$) was used to prevent spurious causal influences due to the low temporal resolution and hemodynamic blurring in the fMRI signal and to eliminate redundant bidirectional connections in the network. The order of the autoregressive model used for computation of the influence measure was set to 1, based on exploratory analyses using the Bayesian information criterion (Seth, 2005). We performed statistical inference on the causal connections using bootstrap analysis: block-randomized time courses were used to generate an empirical null distribution of causal links (as in Roebroeck et al., 2005). Finally, causal influences across subjects were entered into a nonparametric analysis (Wilcoxon signed-rank test at the $p < 0.05$ level) to determine significant directions of influence between ROIs across subjects.

Supplemental Data

The Supplemental Data for this article can be found online at <http://www.neuron.org/cgi/content/full/55/3/521/DC1>.

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